

Problem Set 3 solution

Issued: Day 6

Due: Day 8

(20 pts total)

BE.462J/3.962J

Spring 2003

A recent study of controlled release of a model small-molecule drug from poly(lactide-co-glycolide) microspheres prepared by the single-emulsion method found that the diffusion constant of the drug through the polymer was best related to the polymer's molecular weight according to:

$$D(t) = D_0 + \frac{\square}{M(t)}$$

In this equation, \square and D_0 are constants, and $M(t)$ is the molecular weight of the matrix polymer. From data obtained on PLGA microspheres, the constants were determined to be:

$$\square = 2.1 \times 10^{-11} \text{ cm}^2(\text{kg/mole})/\text{s}$$

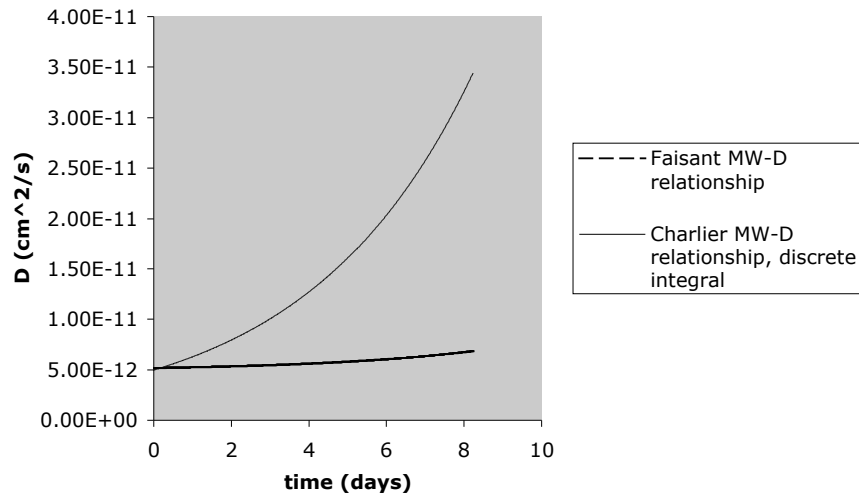
$$D_0 = 4.9 \times 10^{-12} \text{ cm}^2/\text{s}$$

We can use this expression for $D(t)$ in the Charlier controlled release model to obtain modified expressions for $h(t)$ and $Q(t)$ (we'll call this model B, and the expression derived in class model A). Assume that the molecular weight $M(t) = M_0 e^{-kt}$, where M_0 is the initial molecular weight and k is the degradation rate constant for PLGA hydrolysis. A reasonable estimate for k is:

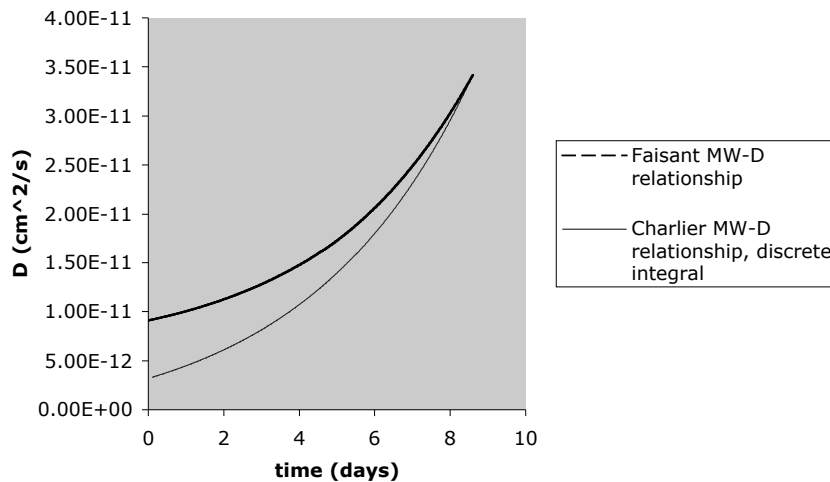
$$\text{Degradation rate constant for PLGA hydrolysis: } k = 9.8 \text{E-}03 \text{ hr}^{-1}$$

1. (5 pts) Quantitatively, will the diffusion constant in model B given above differ significantly from that obtained from model A derived in class over experimentally-relevant timescales?

The difference in diffusion constants depends significantly on the initial value of the molecular weight, M_0 . For release from a high molecular weight matrix with $M_0 = 80,000 \text{ g/mole}$, we have:



...where the diffusion constant starts similar in both models and becomes greatly disparate after several days of hydrolysis. In contrast, if a low molecular weight matrix is used (e.g., the plot below is for $M_0 = 5000$ g/mole), the diffusion constant begins quite disparate and becomes similar in each model after several days:



This analysis indicates that for a high molecular weight matrix, the two models will at least initially predict similar release profiles, which will become different as time goes on (after only 24-48 hours). For a low molecular weight matrix, the difference in release profiles will be apparent immediately.

- (5 pts) Using the model B formula above for the diffusion constant, derive a new expression for the thickness of the diffusion field $h(t)$ in the Charlier model. Assume $M(t)$ has an exponential decay with time as derived in class.

$$D = D_0 + \frac{\Phi}{M(t)}$$

FROM THE CHARLIER MODEL:

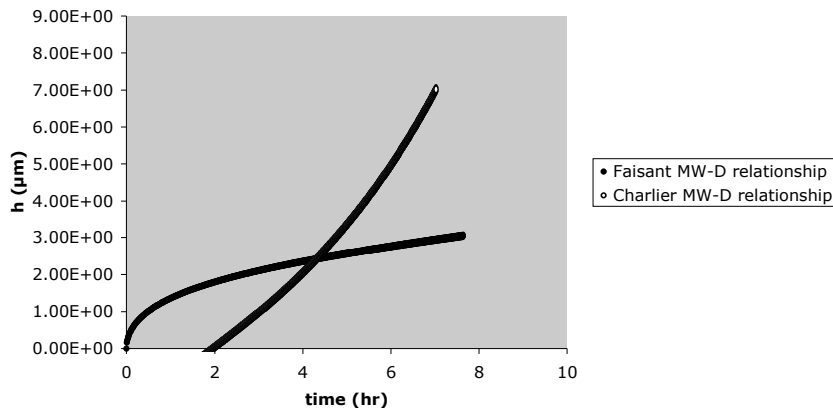
$$D(t) \frac{C_s}{C_0} dt = h' dh'$$

$$\int_0^t \left(D_0 + \frac{\Phi}{M_0 e^{-kt}} \right) \frac{C_s}{C_0} dt = \int_0^h h' dh'$$

$$\frac{C_s}{C_0} D_0 t + \int_0^t \frac{\Phi C_s e^{kt}}{C_0 M_0} dt = \frac{h^2}{2}$$

$$\frac{C_s}{C_0} \left[D_0 t + \frac{\Phi}{M_0} \left(\frac{e^{kt} - 1}{k} \right) \right] = \frac{h^2}{2}$$

$$\therefore h(t) = \left[2 \frac{C_s}{C_0} \left(D_0 t + \frac{\Phi}{M_0} \left(\frac{e^{kt} - 1}{k} \right) \right) \right]^{1/2}$$



3. (10 pts) Using the data above and that given below, determine how long release experiments that measure $Q(t)$ (total amount of drug released at time t) would need to be carried out to distinguish which of the two models for the diffusion constant ($D = D_0 e^{kt}$ as derived in class, or the expression given above) best represents release of HGH from a PLGA matrix in the framework of the Charlier model. (Hint: plot $Q(t)$ for each of the two models; solve for $Q(t)$ in model B by numerically integrating an expression $dQ = (\dots)dt$.)

Solubility of HGH in PLGA matrix: $C_s = 6.12E-04 \text{ g/cm}^3$
 Concentration of HGH encapsulated in the matrix: $C_0 = 0.02 \text{ g/cm}^3$
 Surface area of release matrix: $A = 1.67 \text{ cm}^2$
 Initial molecular weight of the matrix: $M_0 = 78,000 \text{ g/mole}$

AGAIN USING THE CHARLIER MODEL:

$$(i) \quad \frac{1}{A} \frac{dQ}{dt} = \frac{DC_s}{h(t)}$$

REARRANGING:

$$(ii) \quad Q = \int_0^t \frac{ADC_s}{h(t)} dt = \int_0^t C_s A \left(D_0 + \frac{\phi}{m_0 e^{-kt}} \right) \left[\frac{2C_s}{C_0} \left(D_0 t + \frac{\phi}{m_0} \frac{(e^{kt} - 1)}{k} \right) \right]^{1/2} dt$$

... SINCE (ii) IS NOT STRAIGHTFORWARD TO INTEGRATE, WE CAN OBTAIN A REASONABLE NUMERICAL ESTIMATE FOR $Q(t)$ USING (i) INSTEAD:

$$(iii) \quad dQ = \frac{AD(t)C_s}{h(t)} dt$$

↓ DISCRETE INTEGRATION

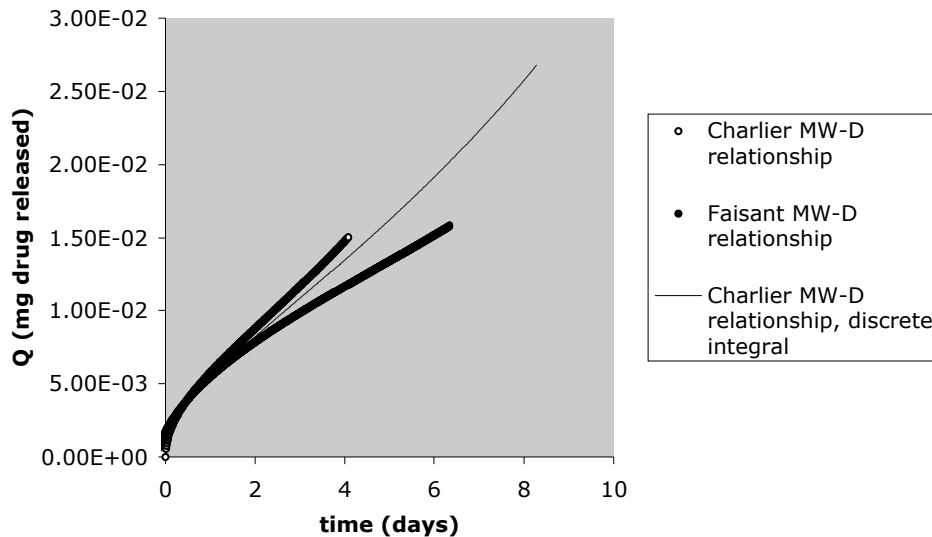
$$(iv) \quad \Delta Q_i = \frac{AD(t)C_s}{h(t)} \Delta t_i$$

WHERE ΔQ_i IS THE AMOUNT OF DRUG RELEASED IN A SMALL TIME INTERVAL Δt_i

AND (v) $Q = \sum_{i=1}^{all} \Delta Q_i$ (Q IS OBTAINED BY SUMMING ALL THE ΔQ_i FROM TIME 0 TO TIME t)

SINCE WE HAVE EXPLICIT EXPRESSIONS FOR $D(t)$ AND $h(t)$, (iv) AND (v) CAN BE IMPLEMENTED IN A SPREADSHEET / MATLAB / CALCULATOR TO NUMERICALLY OBTAIN $Q(t)$ IN MODEL B.

Using the derived expressions, we can compare release predicted by model A and model B:



Thus, for the given parameters, release experiments carried out for at least 2 days would be necessary for the 2 models to deviate from one another significantly. Release experiments carried out for 10 days should allow an unequivocal determination of which model better fits the experimental system.